

# Piezoresistive Elastomer Composites Used for Pressure Sensing

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**Abstract**— Pressure sensors with capability to detect small physical movements and mechanical deformations have been widely used in wearable and medical applications. However, devices that are commercially available currently require complex designs and fabrication and present only a limited force-range sensitivity. To simplify the design, a thermoplastic polyurethane (TPU)/ carbon nanotubes (CNTs) composite film has been developed using a melt extrusion technique followed by compression moulding. Pressure sensors were made from these films, whose piezoresistive response have been analysed as a function of the concentrations of CNTs, around the percolation threshold. The changes in the voltage of the device with applied pressure was continuously measured using a voltage divider system coupled with an electromechanical test machine that dynamically loaded the sensors under compression. The voltage divider system was tuned to obtain the best sensitivity and signal/noise (S/N) ratio for each device tested. The results showed that sensors containing a target of 2.5 wt.% CNTs had market leading sensitivity and repeatability during long-term stability testing and showed high durability during underwater testing indicating that such devices can be used as a promising robust pressure sensitive sensor in wearable devices.

**Index Terms**— Sensor, Piezoresistive, Thermoplastic polyurethane, Carbon nanotubes, Electro-mechanical behaviour.

## I. Introduction

Flexible pressure sensors can be categorized into three main groups including piezoresistive, capacitive and piezoelectric, according to their sensing mechanisms [1,2]. Piezoresistivity, as an important property of the conductive materials, enables them to be particularly promising to be used as pressure sensors due to their simple structure and low cost [2]. This property describes the changes in electrical resistance resulting from a mechanical deformation of the material [3–6]. There are many materials, like inorganic semiconductors and metals that exhibit piezoresistive behaviour, which are used in sensor applications. However, due to their inherent rigidity, their applications are limited, especially in wearable devices [7–9]. Therefore, conductive polymer composites with mechanical flexibility and controllable electrical properties are introduced in development of such a sensor, by integration of conductive fillers such as carbon nanotubes (CNTs) [10–14], graphene [15–17], hybrids of CNTs and graphene [18], carbon black (CB) [14,19–21] and metal nanoparticles [22–24] into a polymer matrix. These discoveries have led to the development of several types of flexible and highly sensitive pressure or strain sensors for different applications, from health monitoring

to wearable devices [25–34]. To achieve a suitable flexibility of the sensor, an elastomer with a high elasticity and a low elastic modulus is typically used as a polymer matrix [35,36]. The most widely selected elastomers in sensor developments are polydimethylsiloxane (PDMS) also known as silicone rubber [37–40], thermoplastic polyurethane (TPU) [13,31,41,42] and rubber [25,43,44].

There are already pressure sensors available in the market, which exhibit good performance in many applications [45,46]. However, their complex design, multi-layered structure, often including several printing steps, limited force-range sensitivity, and finally poor environmental stability, restricts their utilisation in many potential applications.

In this work, a pressure sensor with a simple structure was fabricated based on TPU as a flexible matrix and using CNTs as the conductive network. The conductive composite films were produced through melt extrusion technique using a twin screw compounder, followed by hot pressing into a piezoresistive film layer from which the sensors were cut. The electrical properties of the constructed sensors were analysed using a voltage divider system which adopts an in house developed LabVIEW program. A specified load protocol that

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cyclically loaded the sensor in compression was applied using an Instron ElectroPuls universal test machine, and the force-sensitivity, repeatability, long-term stability, and durability of the sensors were all characterised both in air and when exposed to water. Then, these newly developed sensors were compared to a leading commercial sensor to evaluate their sensing performance, load range sensitivity and long-term durability. The results highlight that the volume fraction of the CNTs in the composite and the selection of suitable reference resistors in voltage divider system were both essential elements when optimising the piezoresistivity response.

The simple and scalable fabrication techniques that were used to develop a durable sensor with high sensitivity at different force range and excellent repeatability, could bring a great potential for these sensors to be used in wearable sensing devices.

## II. MATERIALS AND METHODS

### A. Materials

Thermoplastic polyurethane (TPU), Estane® 58437, an aromatic polyester-based TPU with shore A hardness of  $85 \pm 3$  and density of  $1.19 \text{ g/cm}^3$ , was purchased from Lubrizol. Multi-walled carbon nanotubes (CNTs), NC7000™, with an average length of  $1.5 \mu\text{m}$  and average diameter of  $9.5 \text{ nm}$  were purchased from Nanocyl S.A.

### B. Polymer Compounding

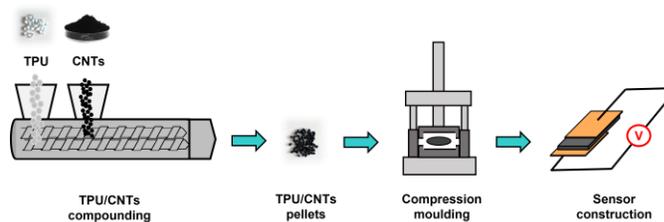
The samples in this work were prepared from a masterbatch of TPU containing a nominal CNTs concentration of 5 wt.%. The masterbatch was prepared using a Collin ZK25 twin-screw compounder with a screw length-to-diameter ratio of 42, screw speed of 200 rpm and a temperature profile from zone 1 to zone 8 (die) of  $190 / 240 / 200 / 200 / 200 / 200 / 200 / 180 \text{ }^\circ\text{C}$ . The main feeder of the ZK25 compounder was used to supply TPU at a speed of  $1.9 \text{ kg/h}$ . The TPU pellets were pre-dried at  $80 \text{ }^\circ\text{C}$  overnight before compounding. The side feeding system was used to supply the as-received CNTs into zone 3 of the compounder at a speed of  $0.1 \text{ kg/h}$ . The extrudate was cooled down in a water bath and pelletised.

The pellets of the masterbatch were then dried at  $80 \text{ }^\circ\text{C}$  overnight before being blended to reduce the CNTs volume fraction with pre-dried, neat TPU and obtain final sample materials with nominal CNTs concentrations of 2.1, 2.3 and 2.5%. The blending was done using an Xplore MC15HT micro-compounder operating in recirculation mode for 3 min in an Argon atmosphere with a screw speed of 200 rpm and a temperature of  $200 \text{ }^\circ\text{C}$ . The extrudates were cooled down in ambient air and pelletised.

### C. Film Preparation and Sensor Construction

TPU/CNTs blend films with different CNTs proportions were prepared using a hot press machine (Collin E300). The temperature was raised to  $185 \text{ }^\circ\text{C}$  and the compounds were kept at this temperature for 3 min without pressure, then 100 bar pressure was applied for 30 s, followed by cooling under the same pressure. An aluminium mould of size  $300 \text{ mm} \times 300 \text{ mm}$  was used to produce films of size  $100 \text{ mm} \times 100 \text{ mm}$ . To construct the sensors, films were cut from the centre into  $20 \text{ mm} \times 20 \text{ mm}$  pieces with an average  $200 \mu\text{m}$  thickness and

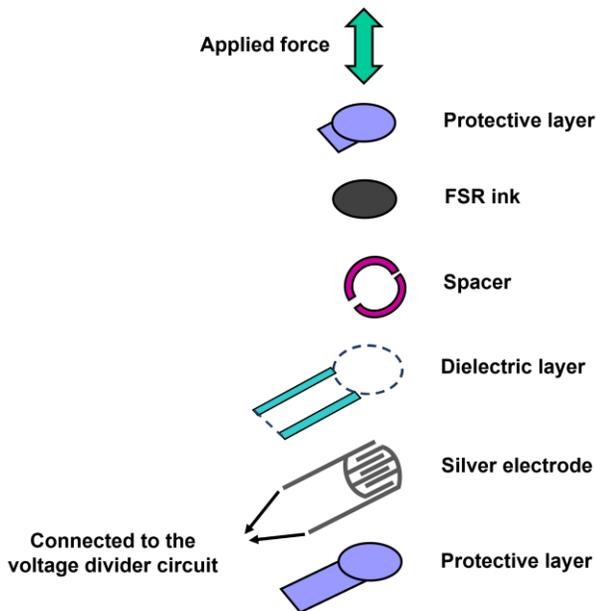
connected to the external wire electrodes using silver paint. The schematic of different steps in sensor fabrication is shown in Figure 1.



Nader1. Schematic of all the steps adopted through sensor construction.

### D. Commercial Sensor Structure

An example of a simplified commercial pressure sensor structure is shown in Figure 2. A force sensitive resistor (FSR) ink is printed through screen printing technique from a liquid and cured to make a solid layer. An adhesive spacer is inserted between the FSR ink and a layer of interdigitated electrodes. The small free volume provided by the spacer allows for air to be vented in and out and reach a pressure equilibrium with the external atmosphere. In this way, the sensor promotes a fast and complete recovery to its initial unloaded state, after each loading cycle through air ventilation. The spacer can also allow for a higher sensitivity at low forces due to the increasing electrical contact between the FSR ink and the interdigitated electrodes as a function of the applied force. A dielectric layer is printed on top of the silver electrode to avoid interference and protect against corrosion. Finally, two outer protective layers, typically made of polyethylene terephthalate (PET) are added to insulate the sensor from the environment. Due to this complex structure that involves several printing steps, and which produces a limited force range sensitivity, the use of these FSR sensors is restricted to a few limited applications. For example, if we consider the case of monitoring human walking and running activities, wearable FSR sensors are required to sense a force within the range of  $0\text{-}100 \text{ N}$ . However, existing commercial sensors do not perform well over this force range and are affected by corrosion at the interdigitated ends and are subject to wearing by the relative sliding between the FSR ink and electrode layers due to the free volume produced by the spacer.



Nader2. Schematic structure of a commercially available sensor.

### E. Characterisation Methods; TGA, SEM

Thermogravimetric analysis (TGA) was used to confirm the CNTs concentrations in the polymer matrix using TA/TGA5500 instrument. The TPU/CNTs blend pellets were heated up from room temperature to 600 °C at a heating rate of 20 °C/min under an inert nitrogen atmosphere. The tests were repeated 3 times for each sample. The actual filler content was estimated from the residual weight percentage at 600 °C, and the results are shown in the supporting information, Figure S1. Scanning electron microscopy (SEM) was utilized to examine the CNT's dispersion in the TPU matrix. SEM images from cross-section were obtained using field-emission scanning electron microscope (FEI Inspect F), OXFORD INSTRUMENTS, with 20 kV acceleration voltage. For cross-section SEM imaging, the polymeric films were cryogenically fractured in liquid nitrogen. Before imaging, the samples were sputter-coated with about a 3 nm gold layer on the fracture surface, to reduce charging effects. To prepare the CNTs sample for imaging, a low concentration of about 10 mg/ mL CNTs was dispersed in ethanol, sonicated for 3 mins, and deposited on a glass slide. After evaporation of ethanol, CNTs were transferred onto a carbon tape and SEM imaging was performed under the same conditions as above.

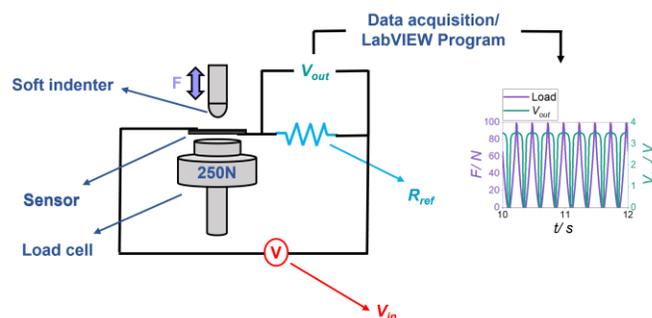
### F. Data Acquisition System

A fundamental circuit widely adopted in electronics is a voltage divider, which produces an output response based on a proportion of its input voltage [5,47]. In this system, a simple and constant known resistor  $R_{ref}$  and the sensor are connected in series, as shown in Figure 3, and attached to a power supply (Rapid DC POWER SUPPLY HY3005D) with a certain input voltage  $V_{in}$  (3.5 V was used throughout this work). As the voltage is distributed between the two resistors, one with a known reference resistance and the sensor with an unknown resistance, the output response  $V_{out}$  would be a function of the

input voltage. As the electrical resistance  $R_{sensor}$  of the piezoresistive material changes as a function of the applied force  $F$ , the measured output voltage  $V_{out}$  of the voltage divider system is also a function of  $F$ :

$$V_{out}(F) = \frac{V_{in} \cdot R_{ref}}{R_{sensor}(F) + R_{ref}} \quad (1)$$

In this work, an Instron ElectroPuls E1000 machine was used to apply different loading profiles on the sensors, while monitoring  $V_{out}$  of a voltage divider system using a NATIONAL INSTRUMENTS USB (NI USB-6009) together with LabVIEW program. A 250 N load cell and a half sphere-shaped soft test indenter made of rubber with 15 mm diameter attached to the actuator were used.

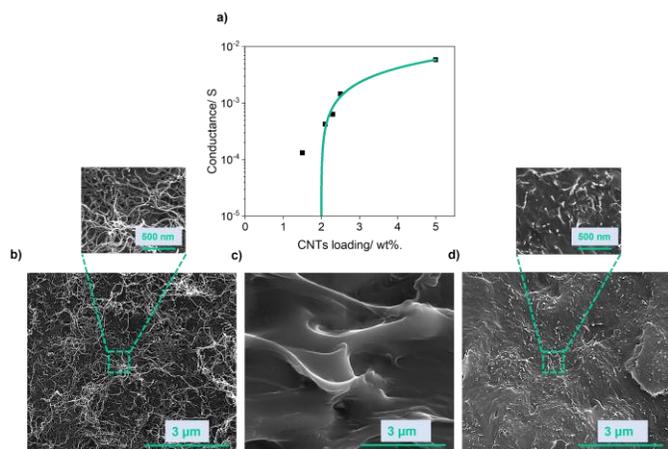


Nader3. Schematic of the sensing measurement set up and data acquisition.

## III. RESULTS

### A. TPU/CNTs Compound Characterisation

Figure 4a shows the percolation threshold trend for CNTs inside the TPU matrix. We estimated the electrical percolation threshold by fitting the conductance values of a series of TPU + x% CNTs composite materials, when a very small compressive force of 0.00063 N was applied to ensure a good contact between the materials and the electrode. We could not measure any conductance for materials containing less than 1.5 wt.% CNTs. Since the samples had the same thickness and the electrode was the same for every sensor, we did not convert the conductance values into conductivities. We fitted the conductance ( $G$ ) of the sensors with the following conductivity model:  $G = G_0 (w - w_c)^n$ , where  $G_0$  is the conductivity of the composite material when the CNTs concentration approaches 100%,  $w$  is the CNTs weight concentration,  $w_c$  is the percolation threshold, and  $n$  is the percolation exponent. We found that the percolation threshold was close to 2 wt.% and the sensors with CNTs loading close to the electrical percolation threshold, were investigated in this work. In this way, any small compressive force would have a dramatic impact on the number of conductive paths, which should allow for very high sensitivities.

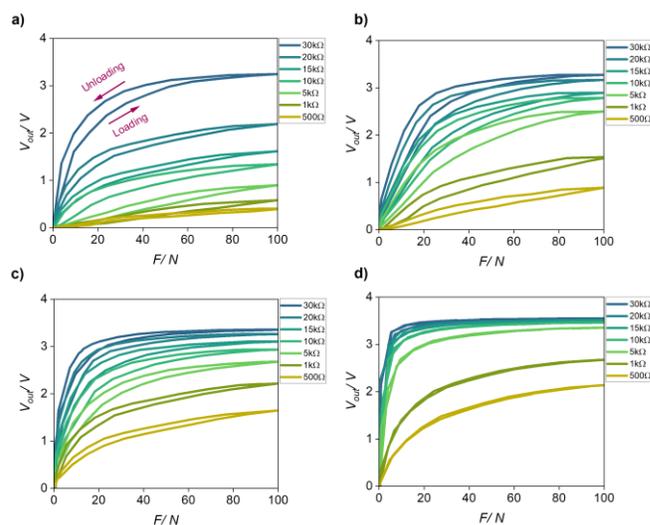


**Nader4.** a) Illustration of percolation threshold of CNTs inside the polymer matrix, b) SEM image of the CNTs dispersed in ethanol, and freeze-fractured cross-sectional SEM image of the c) pure TPU and d) typical TPU/CNTs compound.

SEM imaging was used to investigate the distribution of CNTs in the polymer matrix on a cryogenically fractured cross-sectional surface and the results are displayed in Figure 4d. To have a better understanding of the morphologies, SEM image of the pure CNTs dispersed in ethanol is shown in Figure 4b and a freeze fractured unfilled TPU film is shown in Figure 4c. In general, strong Van der Waals interactions among nanofillers, large surface area and small dimensions are the main parameters that causes the nanoparticles aggregations [48]. The results showed that CNTs are relatively well distributed inside the polymer matrix for all the samples, due to the energetic mixing during melt extrusion, which allowed CNTs to become well dispersed inside the molten TPU matrix.

### B. Output Response Dependence Upon the Reference Resistor

It is a requirement to have the highest signal intensity over a specified force range  $0 < F < F_{MAX}$ . Therefore, a suitable reference resistor with  $R_{ref} > R_{sensor}(F_{MAX})$  should be chosen so that  $V_{out}(F_{MAX})$  approaches the applied voltage  $V_{in}$  (see Equation 1) when the maximum force is applied. On the other hand,  $V_{out}$  is required to increase as linearly as possible with  $F$  to produce increased sensitivity, which is possible only when  $R_{sensor}(F) > R_{ref}$ . These two opposite requirements imply the need to find a good compromise in the value of  $R_{ref}$  used, so that  $V_{out}$  can approach  $V_{in}$  at  $F_{MAX}$  without reaching a plateau at lower forces. To investigate the best reference resistor for our sensors when subjected to a compressive force range of 0-100 N, 50 loading and unloading cycles were performed at 4 Hz using a wide range of  $R_{ref}$  values from 500  $\Omega$  to 30 k $\Omega$ . Figure 5 displays the relation between the applied force range and the sensor output response. For simplicity, only one loading-unloading cycle is shown in Figure 5 for each reference resistor. (The output response over 50 cycles is shown in the supporting information, shown in Figure S2).



**Nader5.** Output voltage,  $V_{out}$  for the a) TPU/2.1% CNTs, b) TPU/2.3% CNTs, c) TPU/2.5% CNTs test materials and d) a commercial sensor with 500  $\Omega$ , 1 k $\Omega$ , 5 k $\Omega$ , 10 k $\Omega$ , 15 k $\Omega$ , 20 k $\Omega$  and 30 k $\Omega$  reference resistors used in the voltage divider system.

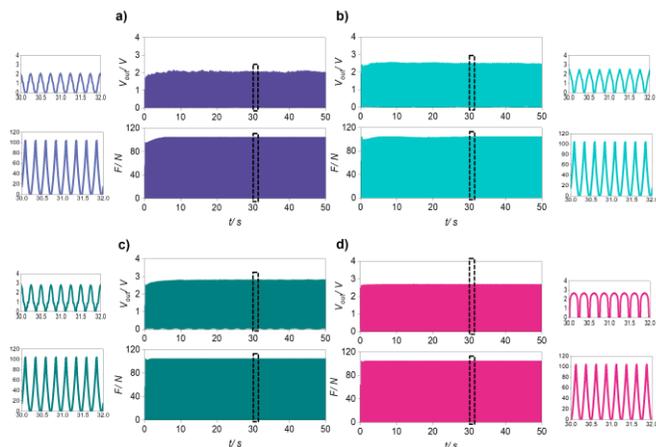
As expected, the intensity of the output response of each sensor is increased when using higher  $R_{ref}$  values. However,  $V_{out}$  could reach a plateau well before the maximum force was applied if  $R_{ref}$  was too high. Instead, when  $R_{ref}$  was small,  $V_{out}$  appeared to increase more linearly with the force, but could reach only small values within the applied force range. From a qualitative analysis of Figure 5, the best  $R_{ref}$  values for TPU/2.1% CNTs, TPU/2.3% CNTs and TPU/2.5% CNTs sensors appear to be 20 k $\Omega$ , 15 k $\Omega$  and 10 k $\Omega$ , respectively. The best  $R_{ref}$  for the commercial sensor appears to be 1 k $\Omega$ .

### C. Sensing Performance During a Cyclic Pressure Loading Analysis

To evaluate the potential of the fabricated compounds to be used as a piezoresistive pressure sensor, the sensors were subjected to a cyclic pressure loading and unloading tests. All measurements were done for 200 cycles at a frequency of 4 Hz and a constant maximum load of 100 N using the optimised  $R_{ref}$  for each sensor. Figure 6 displays the applied load protocol together with the output response in the form of voltage change from the reference resistor in the voltage divider circuit obtained using the in house developed LabVIEW code.

The output response  $V_{out}$  increased with the applied pressure due to the change in the CNTs percolation network of the piezoresistive composites that became better interconnected with more conductive paths [4]. Moreover, as expected from Equation 1,  $V_{out}$  could reach higher values when the sensors contained higher CNTs loadings, because the corresponding sensor resistances decreased.

In addition, the enlarged images indicate very stable responses in the maximum recorded voltages throughout the tests. This reflects the repeatability in the output response of the sensors under cyclic loading.



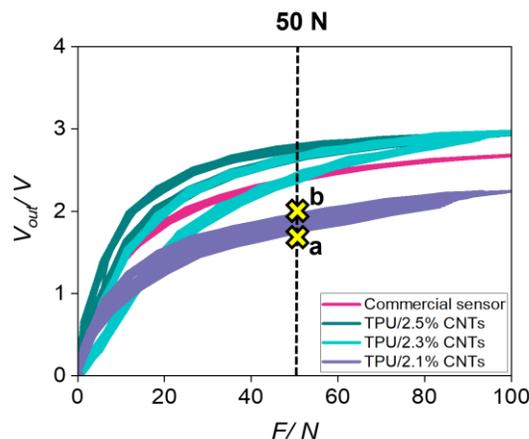
**Nader6.** Applied load and output response for a) TPU/2.1% CNTs, b) TPU/2.3% CNTs, c) TPU/2.5% CNTs and d) commercial sensor during cyclic pressure loading/unloading testing. (The zoomed in region is for 2 seconds to help visualise the shape of the curves).

An important observation is the size of the hysteresis loop in each loading-unloading cycle, where the smallest hysteresis is desirable [2]. This is because a specific output voltage would represent a narrower range of applied force. The electrical hysteresis reflects the normal mechanical hysteresis behaviour of the polymer and the filler-polymer interactions [30,48–52]. Stronger interfacial interactions between CNTs and elastic polymer network would possibly produce lower mechanical hysteresis and perhaps increased reversibility in the sensors [53–56]. In addition, the relaxation behaviour of the polymer matrix could also produce a different loading and unloading response, which will contribute to the mechanical hysteresis loop [4].

To examine more closely the hysteresis and recoverability of the sensors, Figure 7 shows the output voltage of 50 compression loading and unloading cycles when the sensors were connected to their optimum reference resistors as mentioned previously. The hysteresis error of each individual sensor at the midpoint of the graph (at 50 N) was calculated by using Equation 2, where a and b are the output voltage in loading and unloading cycles, respectively.

$$\text{Hysteresis error (\%)} = \frac{(b-a)}{a} \times 100 \quad (2)$$

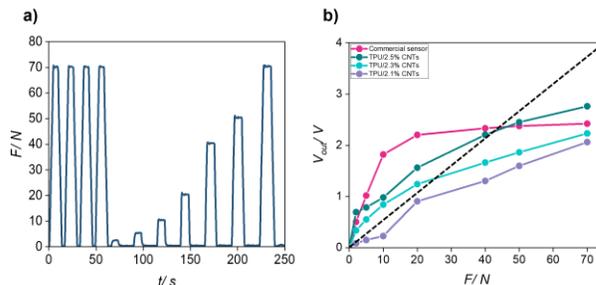
The commercial sensor shows a small hysteresis of about 1.88% and has a good stability after each loading-unloading cycle. Our fabricated sensors, TPU/2.1% CNTs, TPU/2.3% CNTs and TPU/2.5% CNTs, instead, have higher hysteresis of 6.22%, 9.26% and 4.47%, respectively. These sensors also show a signal that is less reproducible after each loading-unloading cycle.



**Nader7.** Output response of 50 loading and unloading cycles on TPU/2.1% CNTs, TPU/2.3% CNTs, TPU/2.5% CNTs devices and the commercial sensor. (To calculate the hysteresis error, two points with letters a and b, at loading and unloading cycles are selected at the midpoint of the graph).

#### D. Sensing Measurement; Force-Sensitivity Characterisation

To understand the force range sensitivity and the best signal-to-noise (S/N) ratio of the sensors, a loading protocol was developed in which the load was increased from 2 to 70 N gradually (Figure 8a). First, all the sensors were subjected to a conditioning cycle, according to which 70 N load was applied four times with 15 N/s rate and kept for 5 s on the sensors, followed by 3 s relaxation time in between. Afterwards, each sensor was tested under the compressive loadings of 2, 5, 10, 20, 40, 50 and 70 N, which were applied for 8 s prior to being released for 17 s. Figure 8b shows the output voltage of the different sensors when connected to their correspondent best reference resistors as determined previously to have their output signals maximised and their sensitivity optimised. For simplicity, the responses of the sensors during the conditioning cycle are not shown in Figure 8b.



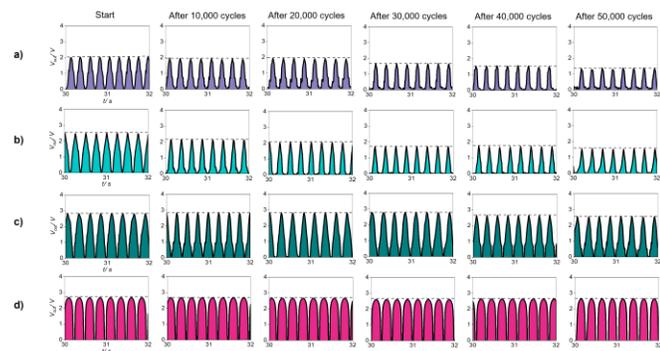
**Nader8.** a) Load protocol diagram applied using electromechanical test machine. b) Output response for the TPU/2.1% CNTs, TPU/2.3% CNTs, TPU/2.5% CNTs and the commercial sensor.

The sensors show different sensitivities over different force ranges. For example, TPU/2.1% CNTs sensor does not show any significant sensitivity for small loads below 10 N, and in contrast, the commercial sensor shows a poor sensitivity for higher loads, between 20 to 70 N. Overall, the output response for TPU/2.3% CNTs and TPU/2.5% CNTs sensors cover a

wider force range (between 5-70 N) and show better sensitivity at each load values.

### E. Long-term Stability Testing

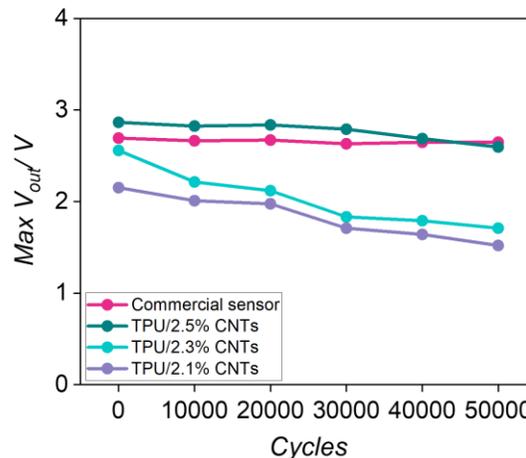
Long-term stability tests were performed up to 50,000 cycles, to assess the performance of the sensors in scenarios relevant to applications as wearable devices and in particular the insoles of smart shoes. A test protocol that would simulate a series of five consecutive walking-and-running sequences was chosen. In the walking phase of each sequence, a 40 N maximum load was applied at a 2 Hz frequency over 10,000 cycles (about 1 h and 20 min). In the running phase, a 100 N maximum load was applied at a 4 Hz frequency over 200 cycles (50 s). The reproducibility of the voltage output during the five running phases is used as a benchmark to assess the quality of the sensors. As a reference, we performed a preliminary running phase before the long-term tests. Figure 8 shows the output voltage from our sensors and the commercial device during the preliminary and the subsequent five running phases (to have a better view of the voltage profiles, only 8 cycles are shown here).



Nader9. Long-term stability test results,  $V_{out}$  per time for a) TPU/2.1% CNTs, b) TPU/2.3% CNTs, c) TPU/2.5% CNTs and d) the commercial sensor.

Figure 10 shows the stability of the maximum output voltage ( $Max V_{out}$ ) during the running phases of the long-term tests. Ideally,  $Max V_{out}$  should remain constant over time to allow for a reliable conversion of the signal into force. This happens with the commercial sensor as well as our sensor containing 2.5% CNTs. In fact,  $Max V_{out}$  of these two sensors decreased only about 2% and 6% over time, respectively. The other two sensors containing 2.1 and 2.3% CNTs show a lower stability as  $Max V_{out}$  decreased about 35% and 39%, respectively. The viscoelastic behaviour of TPU could be the main reason for the decreasing output response during this stability test. This effect is related to the relaxation state of the polymer matrix, which means the polymer matrix does not fully recover its initial state [4], which might be improved by crosslinking the TPU. Better filler-polymer interactions might be another parameter that would introduce a more stable response in TPU/2.5% CNTs sensor. Certainly, the improved performance of the TPU/2.5% CNTs over the TPU/2.1% CNTs and TPU/2.3% CNTs comes from the higher CNTs loading and a resulting better interconnected conductive filler network. The application of repetitive forces over time may break down the CNTs network inside the polymer matrix, which corresponds to increased

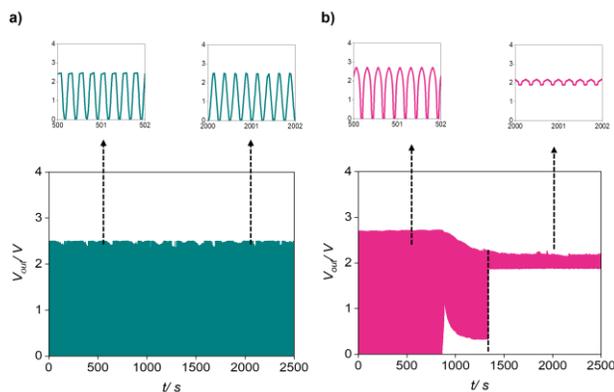
$R_{sensor}$ , hence decreased  $Max V_{out}$ . The smaller the CNTs concentration, the more likely the conductive network deteriorates and the higher  $R_{sensor}$  becomes. At the end, the commercial sensor shows a stable response without any significant change over time, which is a result of the much more complex sensor design.



Nader10. Output voltage variation over time in long-term stability test.

### F. Durability Testing Under Water Ingress

To further evaluate the suitability for wearable applications, the behaviour of the sensors in a wet environment where water could be entered to the sensing area over time was investigated. In this section, only the TPU/2.5% CNTs sensor was compared with the commercial sensor, as it appeared to be the most promising of the sensors tested so far. A protocol of 10,000 loading-unloading cycles at 4 Hz with 100 N maximum force was performed with the sensors being continuously wet by water, which was supplied via a 2-channel Ismatec pump at a flow rate of 1.8 mL/min (the schematic of the testing set-up is shown in Supporting Information, Figure S4). In service the commercial sensor has an air inlet which we simulated by creating a very small hole with a needle near the sensing area, to allow air and water to pass in over time. The results of this experiment are shown in Figure 11a and 11b. The TPU/2.5% CNTs sensor has a much better durability in wet environments compared to the commercial sensor. The baseline of the commercial sensor gradually approaches 1.8 V after about 5,000 cycles, and the sensor loses all its force sensitivity. This probably results from water entering the small free volume present inside the structure as discussed in the introduction and affecting the electrodes, which represents a challenge for these types of application, where the commercial sensor is exposed to outdoor environments. In contrast, our TPU/2.5% CNTs sensor, which was fabricated with a much simpler and cheaper design without any free volume, did not suffer from this problem. Despite displaying some modest variations in the output voltage, the sensing response was much more stable compared to the commercial sensor.



Nader11. Durability test results under water immersion a) TPU/2.5% CNTs and b) commercial sensor.

#### IV. CONCLUSIONS

In this study, a pressure sensor was fabricated by compounding CNTs into a TPU matrix via melt extrusion. A voltage divider system coupled with an ElectroPuls machine were used to apply a compressive load on the sensor and the output voltage of a reference resistor was monitored continuously using an in house designed LabVIEW program. The effect of various CNTs loadings and the use of different reference resistors in the voltage divider system were studied to optimise the design for maximum force sensitivity and lowest signal-to-noise (S/N) ratio. To provide a comparison, our fabricated sensors were compared with a commercial sensor in terms of force range sensitivity, long-term stability, and environmental stability underwater immersion.

The results showed that fabricated sensors have a better sensitivity over a wider force range (5-70 N) compared to the commercial sensor, which showed a poor sensitivity at higher loads (20-70 N). On the other hand, the commercial sensor showed a smaller hysteresis loop of 1.88% during loading-unloading cycles, which reflects its better sensitivity compared to the fabricated sensors, TPU/2.1% CNTs, TPU/2.3% CNTs and TPU/2.5% CNTs, which showed 6.22%, 9.26% and 4.47%, respectively. However, the TPU/2.5% CNTs sensor showed a much better durability when subjected to a water immersion test compared to the commercial sensor. It is worth noting that the TPU/2.5% CNTs sensor displays a better stability during long-term test respect to the other fabricated sensors, indicating that such device can be used as a promising pressure sensor in wearable devices. However, the functionality can be further improved for practical applications, potentially through crosslinking, to decrease the negative impact from viscoelastic behaviour of the polymer, which can influence the hysteresis of the sensor.

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