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3 **ADVANCES IN POPULATION-BASED IMAGING USING**  
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6 **CARDIAC MAGNETIC RESONANCE**  
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*ABSTRACT*

Large population-based studies have helped to identify cardiovascular risk factors and to understand the natural progression of diseases. Cardiac magnetic resonance (CMR) is the reference method for the assessment of ventricular morphology and function given the low variance between scans. In addition, advanced sequences such as MR tagging, T1 mapping, and late gadolinium enhancement allow to assess regional ventricular function and fibrotic changes. MESA was the first study to use CMR on a large scale in a sample of the general population. Subsequent studies focused on cohorts of particular ethnicities or from certain locations with the Jackson Heart Study looking at African-Americans and the Dallas Heart Study at Dallas County Residents. More recently, the German National Cohort and UK Biobank have started to perform CMRs in a significantly larger number of participants (30,000 and 100,000, respectively). The introduction of CMR into prospective cohort studies has allowed to characterize ventricular remodeling in individuals of different age, sex, and gender and has found associations with new environmental exposures. The ability to detect subclinical changes in asymptomatic individuals has also been highlighted by reports of a high number of missed myocardial infarctions (MI) using CMR. In this review, we discuss the use of CMR in the different large population-based studies and compare the various associations found with left and right ventricular structure and function. In addition, we outline automated image analysis strategies aimed at overcoming challenges posed by the large amount of data in population-based studies.

Keywords: CMR; cardiac magnetic resonance; cohort studies; population-based studies

## *INTRODUCTION*

Chronic cardiovascular diseases such as myocardial infarction or heart failure are associated with significant morbidity and mortality. Prospective cohort studies help to identify risk factors associated with the development of those conditions and may allow to characterize high risk individuals for targeted intervention. Early cohort studies such as the Framing Heart Study characterized major cardiac risk factors including smoking[1] and different hypertension phenotypes[2]. More recent studies also include different cardiac imaging techniques including coronary artery calcium scores, echocardiography and cardiac magnetic resonance (CMR)[3,4] in addition to the standardized questionnaires and exams. These approaches have allowed to characterize early changes in cardiac phenotypes and to find novel associations with cardiac risk factors[5]. Further, they have helped to prognosticate long-term outcomes based on specific imaging biomarkers[6].

This review describes the use of CMR across large-scale prospective population studies, highlights novel associations found in the setting of the wide application of those imaging techniques, and discusses novel automated image analysis strategies to overcome challenges posed by the large amount of data obtained in population-based studies.

## *LARGE-SCALE PROSPECTIVE POPULATION STUDIES THAT HAVE USED CMR*

### *Patient selection and follow up*

The first prospective cohort study to use CMR to study cardiac morphology and function was the Multi-Ethnic Study of Atherosclerosis (MESA)[7]. It included a total of 6,814 asymptomatic individuals aged 45-84 who have been followed since 2000-2002[8]. The study included participants of four different ethnicities: Approximately 38% are white, 28% are African-American, 22% are Hispanic, and 12% are Asian. CMR was performed on 5,004 participants at baseline. 3,016 participants also underwent a repeat CMR after approximately 10 years, making it the only large population-based study allowing to study longitudinal changes in cardiac morphology and function. Of note, repeat CMR scans were performed with steady-state free precession (SSFP) cine sequences, while a gradient echo (GRE) cine sequence was used as baseline. The study's CMR protocol is also notable for the additional use of intra-venous (IV) contrast which allowed to better characterize myocardial fibrosis using T1 mapping and late gadolinium enhancement [9]. In addition, MR tagging was performed, a technique that is used to evaluate regional myocardial function.

While MESA included participants of different ethnicities, the Jackson Heart Study investigated cardiovascular disease (CVD) risk factors exclusively in African-Americans, a group with higher rates of CVD and cardiovascular (CV) risk factors than the general population[10]. The study consisted of 5,301 men and women enrolled between 2000 and 2004 [11]. 1,672 participants underwent CMR around 9 years after the baseline visit. Similar to MESA, contrast-enhanced MRI was performed, but only in a subset of individuals with CMR.

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3 The discrepancies between different ethnicities were further studied in the Dallas Heart Study, a  
4 multiethnic cohort which enrolled 6,101 Dallas County Residents between 2000 and 2002 [12,13].  
5 African-Americans were oversampled to represent 50% of the final cohort. CMR was performed  
6 on a sample of 2,971 participants aged 30-65. Of note, the study was later transformed from a  
7 cross-sectional into a longitudinal study and is still ongoing, but CMR has not been repeated.  
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16 The two epidemiological studies with the highest number of participants are the UK Biobank and  
17 the German National Cohort. Both are in their early phases. The UK Biobank recruited more than  
18 500,000 men and women aged 40-69 between 2006 and 2010 in the UK[4]. A random subset of  
19 those participants have been invited back for comprehensive imaging visits including a CMR  
20 examination with the goal to perform 100,000 CMR scans by 2023 [14]. The German National  
21 Cohort is currently recruiting 200,000 participants of the general population aged 20-69. 30,000  
22 randomly selected participants are undergoing whole-body MRI at the baseline visit and possibly  
23 at a follow-up visit 4-5 years later[15,16]. Neither of those studies is performing contrast-enhanced  
24 CMR. The German National Cohort is, however, the only large population-based study that will  
25 use 3 Tesla MRI machines for CMR.  
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41 Other cohort studies that performed CMR include the Study of Health in Pomerania (SHIP)[17], a  
42 study of residents in the German region Pomerania, Age, Gene/Environment Susceptibility  
43 (AGES)-Reykjavik[18], a study of Icelanders, Prospective Investigation of the Vasculature in  
44 Uppsala Seniors (PIVUS)[19], and the Framing Heart Study Offspring cohort[20]. While CMR  
45 scanning has been completed for all of these studies, clinical follow up is still ongoing. Large  
46 cohort studies that are being planned or that are in their very early stages are the Hamburg City  
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Health Cohort Study[21] and the Canadian Alliance of Healthy Hearts and Minds[22]. Further details are summarized in Table 1.

**Table 1.** Large-scale cohort studies (>1,000 participants) that have used CMR.

Study	Population	CMR participants	Time of CMR	CMR protocol	Length of follow up since CMR imaging
MESA[3,7,23]	6,814 asymptomatic men and women (ages 45-84) of 4 different ethnicities without known CVD	Baseline: 5,004 Follow up: 3,016 (completed)	At baseline visit and after ~10 years (2010-2012)	1.5T. LV / RV cine images, MR tagging, LGE, MOLLI, phase-contrast flow images of the ascending aorta, images of the carotid arteries.	Ongoing
Jackson Heart Study[11,24]	5,301 African-Americans (ages 35-84) residing in Jackson, MS	1,672, 600 with IV contrast (completed)	Between 2008-2012 (~8 years after baseline visit)	1.5T. LV / RV cines, MR tagging, contrast sequences, aortic structure and function	Visit 1 2000-2004, visit 2 2005-2008, visit 3 2009-2012
Dallas Heart Study[12]	6,101 Dallas County Residents (ages 18-65). Participants undergoing imaging were ages 30-65.	2,971 (completed)	At baseline visit in 2000-2002	1.5T. LV / RV cines, phase-contrast gradient echo sequence of aorta	Ongoing
UK Biobank[4,25]	>500,000 men and women (aged 40-69) of the general population	Goal 100,000 (ongoing)	Several years following the baseline visit	1.5T. LV / RV cines, MR tagging, aortic flow sequences, native T1, aortic distensibility	Ongoing
German National Cohort[15,16,26]	200,000 men and women (aged 20-69) of the general population	Goal 30,000 (ongoing)	Baseline	3T. LV / RV cines, native angiography, parametric T1 mapping	Ongoing
SHIP[17,27,28]	6,753 men and women (aged 20-79) of the general population of Pomerania	528 contrast-enhanced CMR	2008-2012 (at SHIP-2)	1.5T. LV / RV cines. MRA. LGE in men.	SHIP-0 1997-2001 SHIP-1 2002-2006 SHIP-2 2008-2012 SHIP-3 2014-2016
SHIP-Trend[17,27,28]	4,420 men and women (aged 20-79) of the general population of Pomerania	997 contrast-enhanced CMR	2008-2012 (at baseline visit)	1.5T. LV / RV cines. MRA. LGE in men.	SHIP-Trend 2008-2012 SHIP-Trend-1 Since 2016
Canadian Alliance of Healthy Hearts and Minds[22]	9,700 male and female Canadians aged 35-69	All 9,700 participants	Baseline	Standard CMR: LV / RV cines. Extended CMR: LV / RV cines. MR tagging. Phase-contrast cine. LGE. T1 mapping. T2 star-weighted sensitive sequence.	Ongoing

1 2 3 4 5 6 7	AGES-Reykjavik Study[18]	5,764 Icelanders born between 1907 and 1935	936 as part of the ICELAND MI cohort (completed)	~40 years after initial enrollment in AGES in 1967	1.5T. LV / RV cines. LGE.	Ongoing
8 9 10 11	Hamburg City Health Cohort Study[21]	45,000 inhabitants (aged 45-74) of the city of Hamburg, Germany	12,362 (planned)	Baseline	1.5T. LV / RV cines. LGE. Mapping. Aortic / mitral flow measurements. Angiography. Aortic distensibility.	Ongoing
12 13 14	PIVUS study[19]	1,016 residents in the municipality of Uppsala, Sweden (aged 70 and over)	259 (completed)	3-22 months after primary investigation	1.5T. LV cines. LGE. MRA.	Completed
15 16 17 18 19	Framingham Heart Study Offspring Cohort[20,29]	5,135 residents of Massachusetts, offspring of original FHS cohort	1,837 (completed)	~30 years following initial evaluation	1.5T. LV / RV cines.	Ongoing

20 CMR, cardiac magnetic resonance; CVD, cardiovascular disease; LV, left ventricle; RV, right  
 21 ventricle; LGE, late gadolinium enhancement; MOLLI, modified Look-Locker inversion  
 22 recovery; IV, intra-venous; T, Tesla; SHIP, Study of Health in Pomerania; AGES, Age,  
 23 Gene/Environment Susceptibility; PIVUS, Prospective Investigation of the Vasculature in Uppsala  
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### *CMR imaging and power of study*

There are three factors that affect the power of the study: (i) prevalence of exposure, (ii) prevalence / incidence of outcome, and (iii) number of CMR scans performed. While the number of CMR scans is readily available, the former two factors might easily be overlooked.

The closer the prevalence of the exposure and outcome is to 50%, the higher is the power of the study. This becomes important when looking at the different research questions cohort studies using CMR have tried to answer. Most studies focus on either cardiac structure and function as outcome parameters and try to determine which cardiac risk factors are associated with different cardiac phenotypes, or they try to find imaging biomarkers that are associated with the future outcome of the patient (using cardiac structure and function as assessed by CMR as exposure). Certain cardiac risk factors such as hypertension may be present in up to 40% of the population [30], making it relatively easy to find associations with CMR outcomes. Clinical outcomes such as myocardial infarction may, however, only occur in <1% of the population per year[30], requiring either a higher number of CMR scans or a longer follow up. Tables 2 and 3 show the lowest odds ratios (OR) that are detectable with a power of 80% by the prevalence of the exposure and the number of CMR scans performed as part of the study.

For Table 2, the prevalence of the outcome was assumed to be 4%, while it was assumed to be 2% for the calculations in Table 3. So far, the largest study that has been completed remains the MESA study with 5,000 CMR scans. When investigating the association between a risk factor such as diabetes mellitus, which has been found to be present in approx. 2.5% in the general population[31], and an imaging marker that is present in approximately 4% of the general population, the lowest OR the MESA study could detect would be 2.61, whereas the UK Biobank



will be able to detect an OR as low as 1.30. Even more pronounced are the differences when it comes to associations between CMR findings and long-term clinical outcomes. When investigating an association between an imaging biomarker that is present in 2.5% of participants and a cardiovascular outcome such as myocardial infarction, the lowest detectable OR of the MESA study and the UK Biobank would be 3.36 and 1.43, respectively. Those calculations assume that 2% of participants have had a myocardial infarction (MI). The power of the study can be increased through longer follow-up periods, although at a risk of selection bias due to drop out.

**Table 2.** Lowest detectable OR with a power of 80% assuming a baseline prevalence of the outcome of 4%.

	Prevalence of exposure			
# of CMR scans	2.5%	5%	10%	20%
1,000	5.62	3.93	3.00	2.43
2,000	3.87	2.88	2.30	1.95
5,000	2.61	2.09	1.77	1.56
10,000	2.07	1.74	1.52	1.39
30,000	1.58	1.41	1.29	1.22
100,000	1.30	1.22	1.16	1.12

OR, odds ratio; CMR, cardiac magnetic resonance.

**Table 3.** Lowest detectable OR with a power of 80% assuming a baseline prevalence of the outcome of 2%.

# of CMR scans	Prevalence of exposure			
	2.5%	5%	10%	20%
1,000	7.88	5.38	3.99	3.15
2,000	5.25	3.78	2.92	2.39
5,000	3.36	2.59	2.11	1.81
10,000	2.55	2.06	1.75	1.55
30,000	1.83	1.58	1.41	1.31
100,000	1.43	1.30	1.22	1.16

OR, odds ratio; CMR, cardiac magnetic resonance.

### *ASSOCIATIONS WITH LV STRUCTURE AND FUNCTION*

The relationship of sex and age with CMR based outcomes has been widely studied across the different cohorts. Among individuals without overt cardiovascular disease, male sex has repeatedly been linked to greater left ventricular (LV) volumes and mass. LV ejection fraction (EF) has, however, consistently been found to be higher in women than in men [20,32–34]. While the results of different cohorts indicate that LV volumes decrease with age [32,34,35], striking differences are seen between cross-sectional and longitudinal changes in LV mass: In the cross-sectional analysis of the UK Biobank, no association was seen between age and LV mass [32], findings similar to those in the SHIP study [27]; a cross-sectional analysis of the baseline data of MESA found an inverse relationship between age and LV mass [36]; and a longitudinal increase in LV mass was seen between the MESA baseline and follow up visits [37].

One possible explanation is that those differences are due to selection bias given that only individuals without overt cardiovascular disease at baseline were included in the MESA study - older participants without cardiovascular disease at baseline are likely different from younger participants as they had to be able to remain healthy despite a longer exposure to cardiovascular risk factors. While a longitudinal analysis of the Framingham Heart Study also found an increase in LV mass in men using echocardiography, it also found a longitudinal increase in LV mass in women [38], further complicating the interpretation of the results and also highlighting difficulties when comparing CMR to – especially 2D – echocardiography. Physiologically, a follow-up study provided some insight into potential mediators of the effect of age on LV mass: Subramanya et al. [39] found that higher free testosterone levels and lower sex hormone binding globulin levels (i.e. more androgenic profiles) were associated with higher LV mass in both men and women.

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3 Independently of the cause of the intriguing LV mass findings, it seems clear that LV mass to  
4 volume ratio (LVMR), a marker of adverse remodeling [40], increases over time.  
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9 MESA's unique design makes it ideal for comparisons of different ethnicities. LV mass and  
10 volumes were lower among Asian Americans compared to white Americans, African Americans,  
11 and Hispanics for both men and women [33]. In addition, Hispanics were found to have a higher  
12 prevalence of both concentric and eccentric LV remodeling and LV hypertrophy (LVH). The  
13 association with LVH remained significant for Mexican-origin and Caribbean-origin Hispanics  
14 even after adjustment for all covariates including a higher proportion of elevated blood pressures  
15 [41]. The different population-based studies have also allowed a detailed analysis of the effect of  
16 various CVD risk factors on the cardiac structure and function among the different cohorts. Using  
17 the Jackson Heart Study, Kamimura et al. [42] recently demonstrated the deleterious effect of  
18 cigarette smoking on LV mass and function among African Americans. Similar findings have been  
19 described in the UK Biobank [43] and MESA [44].  
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36 Many of the other traditional CV risk factors and their associations with CMR parameters in  
37 population cohort studies have been reviewed previously [44,45]. Notably, cohort studies using  
38 CMR were able to extend prior reports by demonstrating that various inflammatory markers are  
39 associated with worse cardiac function [46]. High-sensitivity CRP [47], homocysteine [48], and  
40 fibrinogen [49] were associated with systolic myocardial function even in asymptomatic  
41 individuals, emphasizing the role of inflammation in the pathogenesis of cardiac dysfunction.  
42 Several other inflammatory markers including IL-6, soluble thrombomodulin, Factor VIII, and  
43 vWF have been found to be associated with LV mass [46]. Of note, in this MESA study elevated  
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3 CRP and IL-6 were negatively associated with LV mass after adjustment for obesity, indicating a  
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10 A unique advantage of the large cohorts lies in the ability to study associations between  
11 environmental exposures and precise and reproducible CMR measurements. One UK Biobank  
12 study sought to examine the relationship between ambient air pollution and cardiac structure and  
13 function in 3,920 individuals free from pre-existing CVD [50]. Spatial variations of average annual  
14 concentrations of particulate matters of different sizes, nitrogen dioxide, and nitrogen oxides were  
15 calculated for the participant's home addresses. The adjusted analysis was notable for a significant  
16 association between higher concentration of particulate matter and larger ventricular volume  
17 (changes that have been linked to a higher risk of heart failure [51]) with the results indicating that  
18 the association was predominantly driven by finer particles. A similar association was found for  
19 nitrogen dioxide, but not for nitrogen oxide. The study highlights how CMR can be used in  
20 population-based studies to discover biological pathways and to identify high-risk populations.  
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36 More recently, population-based cohort studies have also helped to understand cardiac side effects  
37 of commonly used medications. One MESA study examined the association between H2 receptor  
38 antagonists and changes in LV morphology [52], a relationship that had previously mostly only  
39 been studied in animal models. Another MESA study looked at new statin use and cardiac  
40 remodeling [53] and a UK Biobank study evaluated the impact of menopausal hormone therapy  
41 (MHT) in post-menopausal women free of CVD [54]. Compared to non-users, H2 receptor  
42 antagonist users had fewer detrimental changes in LV parameters. They had a smaller decline in  
43 LV volumes, a smaller decline in LV stroke volume, and a smaller increase in mass/volume ratio.  
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54 Similarly, new statin therapy was associated with less progression of LV mass index and  
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3 mass/volume ratio, though the effects were small in magnitude. The effect sizes increased as the  
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5 statin dose increased. MHT>3 years was associated with significantly smaller ventricular volumes  
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7 and stroke volumes. As described above, smaller ventricular volumes may be associated with more  
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9 favorable outcomes.  
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### *CMR TAGGING AND STRAIN ANALYSIS*

CMR tissue tagging allows to quantify parameters of cardiac physiology such as myocardial strain, strain rate, and torsion [55]. Strain represents either segment shortening (longitudinal or circumferential strain) or thickening (radial strain) and is typically expressed as the fractional change from the original dimension. Temporal integration of strain rate is used to calculate regional strain. Strain rate, a rate of change of deformation, is derived as a spatial derivative of velocity. Circumferential strain is often measured separately at the base, mid-segments, and the apex. Torsion describes the relative rotation of short-axis sections between diastole and systole [55]. While several population-based cohort studies are planning to include tagging, so far only MESA has been used to examine associations with risk factors, cardiac structure, and long-term outcomes [56] as described in a review by Yoneyama et al [44].

CMR tagging in MESA has provided further insight into longitudinal changes in cardiac function. As detailed above, while ventricular volumes increase in both sexes, LV mass increases longitudinally in men, but decreases longitudinally in women. In contrast, the association with LV circumferential strain is the opposite (it decreases longitudinally in men and increases in women) [57]. Torsion was found to increase with age in both sexes and could be an important compensatory mechanism to counter remodeling and maintain global systolic function.

Notably, in addition to insights into the physiology behind alterations in strain patterns, the study [57] highlights another important issue: the need for similar investigations in different population-based studies even if the individual cohorts are large and reliable techniques such as CMR are used. This is illustrated by another positive finding in the study: A V-shaped relationship between change in LV mass/volume ratio and change in torsion, a rather new and not immediately intuitive

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3 finding. The findings are difficult to interpret because of the use of non-standard measure of  
4 torsion. Rather than twist per unit length of the ventricle which doesn't scale appropriately between  
5 hearts of different sized, the torsional shear angle or shear strain should be calculated [58]. In  
6 addition, the p-value of those results is 0.02 and therefore reaches statistical significance based on  
7 the standard 0.05 cutoff. In reality, however, it is almost entirely unclear what those results actually  
8 mean. Using a Bayesian approach, it can be shown that it all depends on the prior probability and  
9 that even if we assume that to be close to 50% in the absence of comparable cohort studies, the  
10 final probability of a true null is well above 10% (and in practice likely even higher than that) [59].  
11 The abundance of observable associations should therefore always be viewed cautiously,  
12 especially in the absence of comparable analyses from other cohorts.  
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### *ADDITIONAL BENEFIT OF IV CONTRAST IN POPULATION-BASED STUDIES*

In addition to classic applications such as angiography, IV contrast allows for the identification of myocardial fibrosis. Post-contrast T1 mapping, a relatively new technique, has been used to assess diffuse interstitial fibrosis, a marker of cardiac remodeling [60]. Post-contrast T1 mapping detects extracellular volume (ECV) expansion [61], a finding that can be associated with a variety of conditions including myocarditis, which lead to myocardial edema [61]. However, in the absence of these pathologies, it can be presumed that ECV expansion is the result of increased interstitial fibrosis [62].

While several different post-contrast T1 mapping sequences exist, the modified Look-Locker inversion recovery (MOLLI) sequence has been used most widely in population-based studies using CMR [63,64]. The findings in MESA that women tend to have higher ECV fractions and that CMR parameters suggestive of fibrosis tend to be associated with older age [64] have previously been summarized [44]. Notable additional findings include the inverse associations between extracellular expansion and ventricular volumes, mass, and reduced circumferential strain in men and women (torsion and LV EF were only negatively associated in men, whereas strain rate was only inversely associated in women) [63]. More recently, a borderline significant association was found between inflammatory markers IL-6 and CRP and diffuse fibrosis in men [65], while no association was found between the extent of LV trabeculation and markers of diffuse fibrosis [66].

Late gadolinium enhancement on the other hand can be used to detect focal myocardial fibrosis and the anatomical pattern can be used to differentiate ischemic from non-ischemic etiologies [67].

This technique has been used in the ICELAND-MI cohort to detect unrecognized myocardial

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3 infarction [18]. More recently, Shanbhag et al. [68] extended those prior findings by also  
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5 investigating the prevalence of non-ischemic myocardial fibrosis. In their study, 23.4% of  
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7 participants had radiologic evidence of a prior MI, while major and minor non-ischemic patterns  
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9 of fibrosis were seen in 6.0% and 26.4%, respectively. Compared to patients with prior MI, non-  
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11 ischemic fibrosis was associated with a higher LV mass, but a lower coronary artery calcium score  
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13 and a lower prevalence of diabetes type II. Interestingly, while the prevalence of recognized and  
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15 unrecognized myocardial infarction in ICELAND-MI was very similar to prior findings in PIVUS  
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17 [69], it was much higher than that in MESA [70]. These differences may be due to demographics  
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19 (ICELAND-MI participants were older with a higher prevalence of cardiac risk factors) and the  
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21 study design (MESA excluded individuals with baseline clinical cardiovascular disease).  
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28 In addition to identification of fibrosis, CMR with IV gadolinium allows for myocardial perfusion  
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30 imaging, a technique that allows to reliably detect coronary artery disease (CAD) when compared  
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32 to other non-invasive imaging modalities [71] as well as invasive studies including coronary  
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34 angiography and fractional flow reserve [72]. Perfusion CMR was performed in a subset of the  
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36 MESA patients at rest and during adenosine-induced hyperemia to determine the perfusion reserve  
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38 (the ratio of myocardial blood flow during hyperemia to rest)[73]. In a MESA study of participants  
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40 without known coronary heart disease (CHD), several well-known risk factors of CHD, including  
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42 hypertension and higher LDL cholesterol, were associated with lower perfusion reserve [73].  
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44 These findings were extended by another study showing that higher coronary artery calcium scores  
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46 are inversely correlated with perfusion reserve, again population-based imaging can help  
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48 identifying subclinical disease and high risk individuals [74], an implication further corroborated  
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50 by the finding that lower perfusion reserve is associated with decreased regional systolic function  
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52 even in asymptomatic participants [75].  
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### *IMAGING BIOMARKERS AND OUTCOME PREDICTIONS*

MESA, ICELAND-MI, and the Framingham Heart Study have studied clinical outcomes following CMR. It has repeatedly been shown that an elevated LV mass and LVH are associated with incident heart failure, coronary heart disease, and cardiovascular death [76–78], a finding that is in line with prior studies using echocardiography [79]. Conversely, a normal CMR has been associated with a lower risk of incident heart failure [80]. Peters et al. [81] recently extended prior reports by showing that individuals with LVH and positive serum biomarkers of myocardial strain constitute the group at highest risk for new asymptomatic LV dysfunction, heart failure, and cardiovascular death.

Interestingly, despite the differences seen in cardiac remodeling over time between men and women as detailed above, the association of LV mass or LV mass/volume with incident cardiovascular disease did not differ between men and women [77]. There is, however, evidence for racial differences. Akintoye et al. [82] found that the relationship between LV mass and incident cardiovascular disease was strongest among Chinese and Hispanics, and weakest for non-Hispanic Whites.

An analysis of the Framingham Heart Study Offspring Cohort [78] showed, similar to the MESA studies, that higher LV mass is associated with a higher incidence of cardiovascular disease. LV wall thickness was also associated with the clinical outcomes in that study, while LV wall/volume ratio was only borderline significant. Further, the study highlighted how, in addition to trying to find causal relationships, large population-based studies that use advanced imaging techniques can improve the prediction of clinical outcomes, an application that has also been described using MESA [83].

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5 More recently, CMR tagging, late gadolinium enhancement, and T1 mapping as described above  
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7 have also been associated with clinical outcomes [68,84,85]. An ICELAND-MI study [68]  
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9 examined the association of ischemic and non-ischemic myocardial fibrosis identified using late-  
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11 gadolinium enhancement and heart failure hospitalization and death from any cause. Patients with  
12  
13 an MI had, on average, a higher amount of fibrosis. Despite this, the group with major non-  
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15 ischemic fibrosis had the highest rates of heart failure hospitalizations compared to patients with  
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17 ischemic fibrosis, minor non-ischemic fibrosis, or no fibrosis after adjustment for confounders.  
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19 The authors highlight the important implication that the pathophysiologic processes leading to  
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21 non-ischemic fibrosis are not captured by the traditional risk factors they adjusted for in the  
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23 analysis.  
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### *ASSOCIATIONS WITH RV STRUCTURE AND FUNCTION*

One of the biggest strengths of CMR is its ability to accurately characterize the right ventricle (RV), which has made it possible to investigate risk factors associated with RV dysfunction and remodeling: Cross-sectional analyses of the Framingham Heart Study Offspring Cohort [86] and MESA [87] have shown that RV mass decreases with age and that men have greater RV mass and larger RV volumes, but lower RV EF. Aaron et al. [88] demonstrated that physical activity is associated with higher RV mass and volume. And while obesity has also been found to be associated with higher RV mass and volume [89], the RV EF was lower in obese than in lean individuals.

One of the risk factors specifically linked to RV dysfunction is pulmonary dysfunction. While it has been known from other cohort studies that chronic pulmonary disease is associated with a higher rate of adverse cardiac outcomes [90], population-based studies using CMR have helped to identify underlying pathways and to characterize subclinical changes in cardiac structure and function. One MESA study sought to examine the association of emphysema with RV changes using the lung density on cardiac CT scans to determine the severity of the emphysema [91]. Greater percent of emphysema was associated with lower RV end-diastolic volume, stroke volume, cardiac output, and mass. The magnitude of those changes was greater among current and former smokers compared to never smokers. Thomson et al. [92] extended those findings by showing that reduced forced expiratory volume (FEV<sub>1</sub>) and forced vital capacity (FVC) are associated with lower RV end-diastolic volume, end-systolic volume, and lower stroke volume in a sample of the UK Biobank cohort without known cardiorespiratory disease.

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3 Similar to the LV, the RV structure and function has also been associated with several commonly  
4 used medications. Histamine 2 (H2) receptor antagonists were associated with a lower RV mass  
5 and smaller RV volume, while the ejection fraction was unchanged [93]. These results remained  
6 significant after adjustment for left ventricular mass, indicating a potential favorable effect on RV  
7 morphology that is independent of the effect on the LV described above. Selective serotonin  
8 reuptake inhibitors (SSRIs), on the other hand, have been found to be associated with larger RV  
9 stroke volume without a change in RV EF [94]. Interestingly, RV mass and RV end-diastolic  
10 volume were higher in men on SSRIs, a finding that is unexpected given a the expected protective  
11 effect of SSRIs against serotonin induced pulmonary hypertension [95]. The cross-sectional design  
12 and lack of adjustment for length of therapy, however, are considerable limitations. The  
13 association between angiotensin converting enzyme (ACE) inhibitors or angiotensin receptor  
14 blockers (ARB) and RV structure and function remains similarly unclear. While a MESA study  
15 found significant associations with RV mass and volumes [96], the study failed to adjust for the  
16 high number of tests performed and adjusted for LV measures which are possibly on the causal  
17 pathway given the known effect of ACE inhibitors and ARBs on LV morphology and function.  
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3 *NOVEL APPROACHES TO IMAGE ANALYSIS – AUTOMATION IN POPULATION-BASED*  
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5 *STUDIES*  
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7 A major challenge for population-based studies is the analysis of the large amount of imaging data.  
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9 The analysis of the CMR scans in clinical practice and the population-based studies discussed  
10 above heavily relies on manual approaches to identify cardiac chambers and blood vessels. This  
11 process is prone to subjective variation and is very time-consuming, requiring up to 30 minutes for  
12 a single CMR analysis of the left and right ventricular volumes. However, population-based studies  
13 may at the same time offer a solution to the problem by providing large datasets that help to  
14 improve machine learning algorithms. While the overall number of participants is still small  
15 compared to other specialties, population-based studies are currently the closest we can get to big  
16 data in a controlled environment in medical imaging and may allow for the development of  
17 algorithms for data analytics at large. The following sections will discuss the analysis process,  
18 which can be divided into a pre-analytical, an analytical, and a post-analytical part.  
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34 *Pre-analysis quality control*  
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36 Prior to segmentation and measurement of cardiac structure and function, it is necessary to ensure  
37 adequate CMR image quality. Incomplete myocardial coverage, suboptimal angulation or slice  
38 position, motion artefacts due to breathing or arrhythmia, aliasing, and truncation artifacts are  
39 some of the issues that may impair the subsequent analysis [97,98]. Initial image quality  
40 assessment is usually performed by radiographers to ensure that the patient does not leave the  
41 scanner before diagnostically interpretable images have been obtained. However, this process may  
42 be subjective and error-prone, and potentially time consuming [99]. Several studies have aimed to  
43 define standardized criteria for quality control through visual inspection in cardiovascular imaging  
44 using MRI [100,101], but the process remains very time consuming and challenges such as inter-  
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3 and intra-reader variability persist. These issues are further compounded when large amounts of  
4 data are obtained for population-based studies because of different imaging centers involved and  
5 a lag in time between image acquisition and analysis [102].  
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12 In an effort to overcome these limitations, Zhang et al. [102] recently proposed an algorithm for  
13 the automatic assessment of full left ventricular coverage. The method was validated in 5,000  
14 CMR scans from the UK Biobank. The algorithm's error rate was just below 5% and demonstrated  
15 good agreement with a human expert. Tarroni et al. [103] proposed a strategy based on the  
16 identification of cardiac landmarks (apex and mitral valve) to estimate heart coverage that was  
17 able to identify cases in the UK Biobank with insufficient coverage with 88% sensitivity and 99%  
18 specificity. In addition, their quality control algorithm was designed to assess inter-slice motion  
19 detection and image contrast estimation in the cardiac region. Motion-corrupted cases were  
20 detected with a sensitivity and specificity of 85% and 95%, respectively. The complexity of motion  
21 detection that is caused by respiratory variation alone has been outlined extensively [104,105] and  
22 is one of the areas where further research is needed to improve automated quality control  
23 techniques. Others include identification and correction for suboptimal angulation and slice  
24 position and automated approaches to predicting results from slices that have poor quality of what  
25 the results would have been with good image quality.  
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#### 45 *Analysis*

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47 The analysis part includes the identification, localization, and segmentation of cardiovascular  
48 contours, enabling an automated quantification of the cardiac structure and function. A number of  
49 (semi-) automated LV segmentation algorithms have been described that include a wide range of  
50 different techniques [106–111]. There are, however, only a few studies evaluating segmentation  
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3 algorithms for more advanced techniques such as T1 mapping [112], late gadolinium enhancement  
4 MR images [113,114], aortic stiffness [115], or aortic flow [116]. In addition, most of them have  
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6 been developed in small datasets, limiting their application in clinical practice or population-based  
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8 studies.  
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14 The Siemens InlineVF was one of the first commercially available fully automated LV analysis  
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16 tools and the results of the D13 version are available to researchers as part of the original UK  
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18 Biobank dataset. A study comparing automated analyses using the D13 as well as the advanced  
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20 E11C InlineVF versions to manual assessments [117] showed that the best precision obtainable  
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22 with the automated analysis was about two to three times that of the manual analysis for ventricular  
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24 volumes and mass. The study also highlighted conditions where misdetection is more common: If  
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26 the aorta is very bright or pulsating, if the contrast between blood and myocardium is weak, and if  
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28 the gray level distributions of the different regions cannot be modeled correctly due to unexpected  
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30 intensities and contrast in the images.  
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36 Also using the UK Biobank, Bai et al. [118] recently developed a fully convolutional network to  
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38 analyze the 4,875 CMR studies that have already been annotated by clinical experts. The  
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40 automated analysis closely matched the analysis by clinical experts with Dice metrics  $>0.9$ . The  
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42 mean differences between automated and manual assessment were only 6.9 for LV mass and  $<10$   
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44 mL for all LV volumes. Automated algorithms have also been found to be able to reliably detect  
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46 the localization of the ascending and descending aorta [119], a step that is vital for the calculation  
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48 of aortic distensibility. Compared to the ground truth (established by visual assessment by 13  
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50 observers), the algorithm was able to detect the ascending and proximal descending aorta with an  
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52 accuracy of 99.4% and 99.8%, respectively.  
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3 Novel algorithms may also help to provide tools for better quantification of the myocardial  
4 structure and function. As detailed above, current clinical assessment is mostly limited to  
5 ventricular mass and volume measures. The Cardiac Atlas Project (CAP) is an international  
6 collaboration to provide a population atlas of asymptomatic and pathological hearts [120–122],  
7 which has facilitated the development and sharing of advanced analysis techniques including  
8 statistical shape modeling. MESA contributed data from the baseline examination of 1,991  
9 asymptomatic volunteers. Data has also been contributed from several other studies including  
10 Defibrillators to Reduce by Magnetic Resonance Imaging Evaluation (DETERMINE) [122].  
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23 Studies using the CAP data have shown that shape analysis techniques such as principal  
24 component analysis (PCA) can be used to quantify remodeling due to myocardial infarction  
25 [123,124] or congenital heart disease [125]. These approaches may help with identifying  
26 individuals with a certain pathology and, consequently, those at increased risk for adverse  
27 outcomes. However, the clinical interpretation of PCA shape components is often difficult as they  
28 are not designed to be related to any of the clinical parameters discussed above. Approaches that  
29 relate statistical modeling to clinical remodeling parameters might help to overcome this limitation  
30 [126].  
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43 In addition to currently available segmentation techniques for ventricular or atrial volumes, further  
44 research should focus on the development of highly accurate and precise segmentation tools for  
45 regional systolic function (strain analysis) and vascular analyses such as aortic stiffness measures  
46 and flow quantification. In addition, automated analysis algorithms are needed for advanced CMR  
47 techniques outlined above including late gadolinium enhancement, CMR perfusion, and mapping  
48 (including T1, T2, T2\*, and extracellular volume).  
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3 *Post-analysis quality control*  
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5 Earlier work has relied on visual verification of segmentation results, which becomes impractical  
6 in large population-based studies. In addition to proposing a fully automatic method for initializing  
7 CMR segmentation, Alba et al. [127] proposed one of the first measures to identify incorrect  
8 segmentation without the need for visual assessment. Failure is detected using statistical, pattern,  
9 and fractal descriptors based on features computed on image intensity values of the blood pool and  
10 myocardium. Using CAP for verification, the accuracy of the segmentation quality control reached  
11 96% in both asymptomatic individuals and in individuals with a prior MI.  
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23 Automated quality control in image segmentation has also been applied to the UK Biobank  
24 datasets. Robinson et al. [128] used Reverse Classification Accuracy (RCA) to predict the quality  
25 of segmentation on a case-by-case basis, allowing not only to identify the quality of the  
26 segmentation, but also if the segmentation has failed. The algorithm was also successfully applied  
27 to a large dataset without ground truth and showed good agreement with visual quality control  
28 scores, simulating real life scenarios. A potential limitation of the approach is the runtime of 11  
29 minutes as it limits immediate feedback.  
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**Table 4.** Automation and Quality Control.

	<b>Pre-Analysis Quality Control</b>	<b>Analysis</b>	<b>Post-Analysis Quality Control</b>
Challenges	<ul style="list-style-type: none"> <li>- Incomplete myocardial coverage</li> <li>- Suboptimal angulation</li> <li>- Suboptimal slice position</li> <li>- Motion artifacts</li> <li>- Aliasing</li> <li>- Truncation artifacts</li> </ul>	<ul style="list-style-type: none"> <li>- Automatic quantification of cardiac structure and function</li> <li>- Segmentation algorithms for more advanced techniques (Mapping of T1 / T2 / T2* / extracellular volume, LGE, CMR perfusion, aortic stiffness, aortic flow)</li> <li>- Advanced analysis techniques such as statistical shape modeling</li> </ul>	<ul style="list-style-type: none"> <li>- Verify correct segmentation without need for visual assessment</li> </ul>
Examples of Current Approaches	<ul style="list-style-type: none"> <li>- Automatic assessment of full LV coverage [102]</li> <li>- Assessment of LV coverage based on cardiac landmarks [103]</li> <li>- Assessment of inter-slice motion [103]</li> </ul>	<ul style="list-style-type: none"> <li>- Siemens InlineVF LV analysis tool [117]</li> <li>- Fully convolutional networks for the analysis of LV mass and volume [118]</li> <li>- Statistical shape analysis using the datasets of the cardiac atlas project [123–126]</li> </ul>	<ul style="list-style-type: none"> <li>- Combination of statistical, pattern, and fractal descriptors based on blood pool and myocardium features [127]</li> <li>- Reverse classification accuracy [128]</li> </ul>

LGE, Late gadolinium enhancement; CMR, Cardiac magnetic resonance; LV, Left ventricle.

## FUTURE WORK

CMR in population-based studies offers a unique opportunity to bring together experts from different fields to combine approaches from medicine, epidemiology, engineering, and computer science. Improvements in image analysis, automation, and quality control will help advance our ability to identify cardiac risk factors and to correlate imaging characteristics with clinical outcomes, a process leading to precision medicine that will be most impactful if cohorts are combined and data are shared (Figure 1).

### *Exposures and Clinical Outcomes*

Large population-based studies are ideal to study the effects of rare exposures or exposures that vary considerably among individuals of the target population. An example of this is the combination of cardiac imaging with genetics: In order to be able to identify new genes that are associated with certain cardiac characteristics at a population level, a large number of participants needs to be included. Further examples include various environmental exposures such as traffic, pollution, noise, or stress. In addition, population-based studies may help to show a benefit associated with new technologies aimed at promoting health such as the Apple Watch. Population-based studies using CMR may also allow the identification of unknown cardiac effects of various medications or even the correlation of findings from different imaging techniques. For example, the large number of cardiac and brain MRIs obtained on participants of the UK Biobank might allow to better understand which cerebral changes are associated with alterations in cardiac structure or function. There are many other organ interactions with the heart that are worth exploring in an aging population with increasing multi-morbidity and polypharmacy: e.g. respiratory-cardiac axis, liver-heart axis or bone-heart axis. All of these questions could be answered as soon as MRIs have been obtained on a critical number of participants of the target

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3 population if a cross-sectional approach is used. Other questions that seek to answer which cardiac  
4 phenotypes are associated with certain clinical outcomes such as cardiovascular events, on the  
5 other hand, will require longer follow up periods.  
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### 10 11 *Image Sequences and Analysis*

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14 The large number of study subjects in population-based studies, time consuming manual analyses,  
15 and significant inter-reader variability require the development of highly accurate, automated  
16 segmentation tools for standard measures such as ventricular mass and volume, and for various  
17 advanced CMR techniques including strain analysis, late gadolinium enhancement, CMR  
18 perfusion, and mapping. In addition to conventional segmentation of these sequences, further  
19 development of advanced analysis techniques may allow for a more precise identification of  
20 individual structural and functional characteristics.  
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32 A very promising example of an advanced analysis technique is the extraction of a large number  
33 of quantitative features from digital images. This process, in combination with the storage in  
34 shared databases to facilitate subsequent hypothesis generation or testing, is known as radiomics  
35 [129,130]. While radiomics has thus far mostly been used in the field of oncology [131,132], it  
36 can be applied to many conditions and will undoubtedly help advance precision medicine by  
37 identifying and verifying new imaging biomarkers. The process of radiomics as outlined  
38 previously [129] includes image acquisition, identification of the volume of interest, segmentation,  
39 extraction and qualification of descriptive features from the volume, and population of a searchable  
40 database. Application of radiomics to CMR data on a population level will not only allow to better  
41 characterize subtle changes in the cardiac phenotype which are not immediately obvious using  
42 standard measures such as LV mass or volume, but it will also allow to improve the prediction of  
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3 outcomes and thereby potentially provide the means to identify individuals who are most likely to  
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5 respond to a certain intervention.  
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10 Finally, the large number of datasets may offer the opportunity to develop algorithms to predict  
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12 the results of sequences which were not directly obtained during an MRI scan. For example, early  
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14 synthetic gadolinium enhancement has been shown to agree with conventional late gadolinium  
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16 enhancement for assessing myocardial scar [133], a finding that may allow to shorten CMR  
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18 acquisition time. Further helpful approaches could for example include the prediction of CMR  
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20 perfusion scans if perfusion imaging was not performed.  
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### 23 24 25 *Quality Control*

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27 The challenges associated with quality control are outlined above. Further research may focus on  
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29 the detection of and correction for respiratory motion artifact and suboptimal angulation and slice  
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31 position. In addition, further development of automated quality control of segmentation and other  
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33 analysis results is needed. Quality improvement projects using quasi-experimental designs  
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35 demonstrating the impact of regular automated quality information feedback to radiographers on  
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37 quality of image acquisition could demonstrate the potential of such an approach in population  
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39 studies but also in clinical practice.  
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### 43 44 45 *Data Sharing*

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47 Despite the large number of participants in each individual study, the clinical goals outlined above  
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49 will only be achieved with a multi-cohort approach that not only allows the inclusion of  
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51 participants from different backgrounds, but also facilitates the link of clinical, laboratory,  
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53 molecular, and clinical data. So far, CAP has helped to establish a large-scale, online accessible  
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3 database of CMR datasets with associated clinical data [120]. While extremely important, the total  
4 number of datasets currently included is fewer than 3,000. Therefore, other approaches have been  
5 developed, most notably euCanSHare [134]. EuCanSHare is a joint EU-Canada project to establish  
6 a cross-border data sharing and multi-cohort cardiovascular research platform. It currently aims to  
7 integrate 35 Canadian and European cohorts, making up over 1 million records [134]. Future  
8 efforts should focus on the development of similar platforms for other regions or, ideally, the  
9 integration of other cohort studies within euCanSHare.  
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21 Sharing and reuse of data and interpretations, particularly in the setting of large-scale population  
22 datasets, are, however, surrounded by several challenges. Specifically, data must be Findable,  
23 Accessible, Interoperable, and Reusable, summarized as the FAIR guiding principles recently  
24 agreed upon by different stakeholders at a Lorentz workshop and summarized by Wilkinson et al.  
25 [135,136]. These high-level principles are in line with previous work such as the Joint Declaration  
26 of Data citation Principles [137] or the ‘Data Seal of Approval’ [138], but specifically focus on  
27 machine actionability – the ability of machines to find and use data, thereby supporting its reuse  
28 by individuals[139]. Future efforts to share data and make results reproducible should attempt to  
29 follow this framework and to quantify the level of FAIRness based on 14 defined metrics [140].  
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3 **Figure 1.** Future Work.  
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## 5 **Future Work**

### 6 **Exposures and Clinical Outcomes**

- 7 - Utilize large datasets to identify new risk factors in fields such as genetics
- 8 - Correlate cardiac and non-cardiac imaging findings
- 9 - Characterize cardiac phenotypes at risk of future cardiac events

### 10 **Imaging Sequences and Analysis**

- 11 - Segmentation of advanced CMR techniques including strain analysis, CMR perfusion, and mapping
- 12 - Advanced analysis techniques such as statistical shape analysis
- 13 - Algorithms to predict sequences not directly obtained during an MRI scan

### 14 **Quality Control**

- 15 - Pre analysis: Ensure adequate image quality (motion correction, correction for suboptimal angulation or slice position)
- 16 - Post analysis: Verification of analysis results
- 17 - Quality improvement projects to demonstrate the impact on population studies and clinical practice

### 18 **Data Sharing**

- 19 - Increase power by combining different cohorts using data platforms such as euCanSHare following FAIR framework
  - 20 - Evaluate differences between populations
  - 21 - Identify associations with non-imaging biomarkers
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## CONCLUSIONS

CMR is the reference standard for the assessment of LV and RV anatomy and function. Since the start of MESA in 2000, CMR has been used in several large population-based studies, which has helped to advance our understanding of the effects of various cardiovascular risk factors on myocardial structure and function. The relatively low prevalence of cardiac risk factors and outcomes in a general population, however, requires large sample sizes. Two ongoing studies, the UK Biobank and the German National Cohort, may help to overcome this limitation due to their significantly higher number of CMR scans.

CMR protocols differ between the individual studies. CMR tagging, T1 mapping, and late gadolinium enhancement are not universally performed, but have helped to detect subclinical disease such as missed MI and have been shown to improve prediction of future cardiovascular events.

The reliable and timely analysis of the large number of scans remains an ongoing challenge. While automated analyses have been developed that closely match the performance of clinical experts, further advances are necessary considering the large sample sizes of the currently ongoing large population-based studies.

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